

# Neuroimaging Harmonization: Approaches, Considerations, and Gaps

Emily Dennis, PhD

TBI and Concussion Center, Dept of Neurology, University of Utah

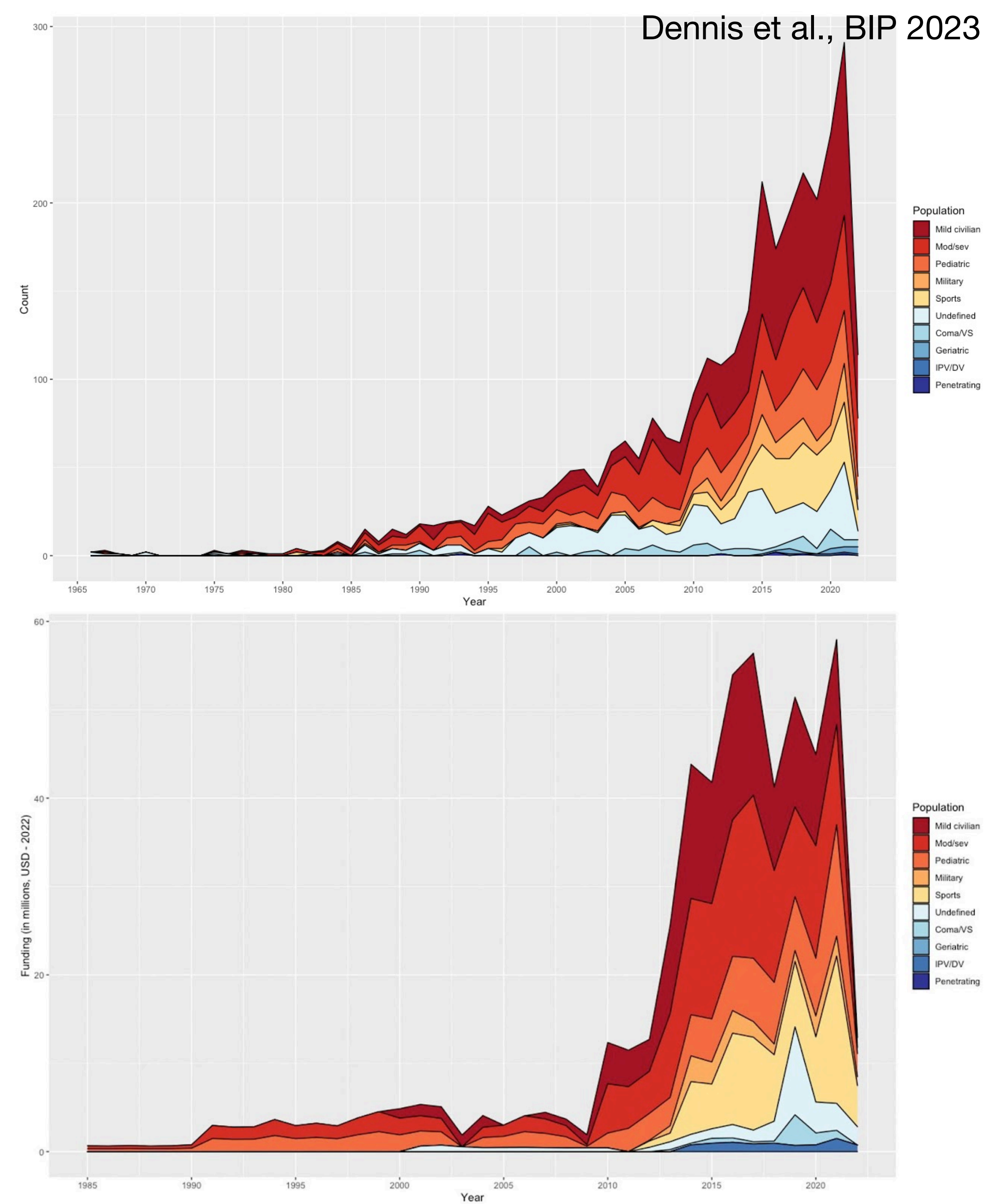
# Goals for today

- Understand the importance of harmonization for neuroimaging data
- Explain types of harmonization and considerations for these
- Review gaps in the field

Focus on neuroimaging in TBI but most approaches and considerations apply to many types of biomarkers across psychiatric and neurological disorders

# Why is harmonization important?

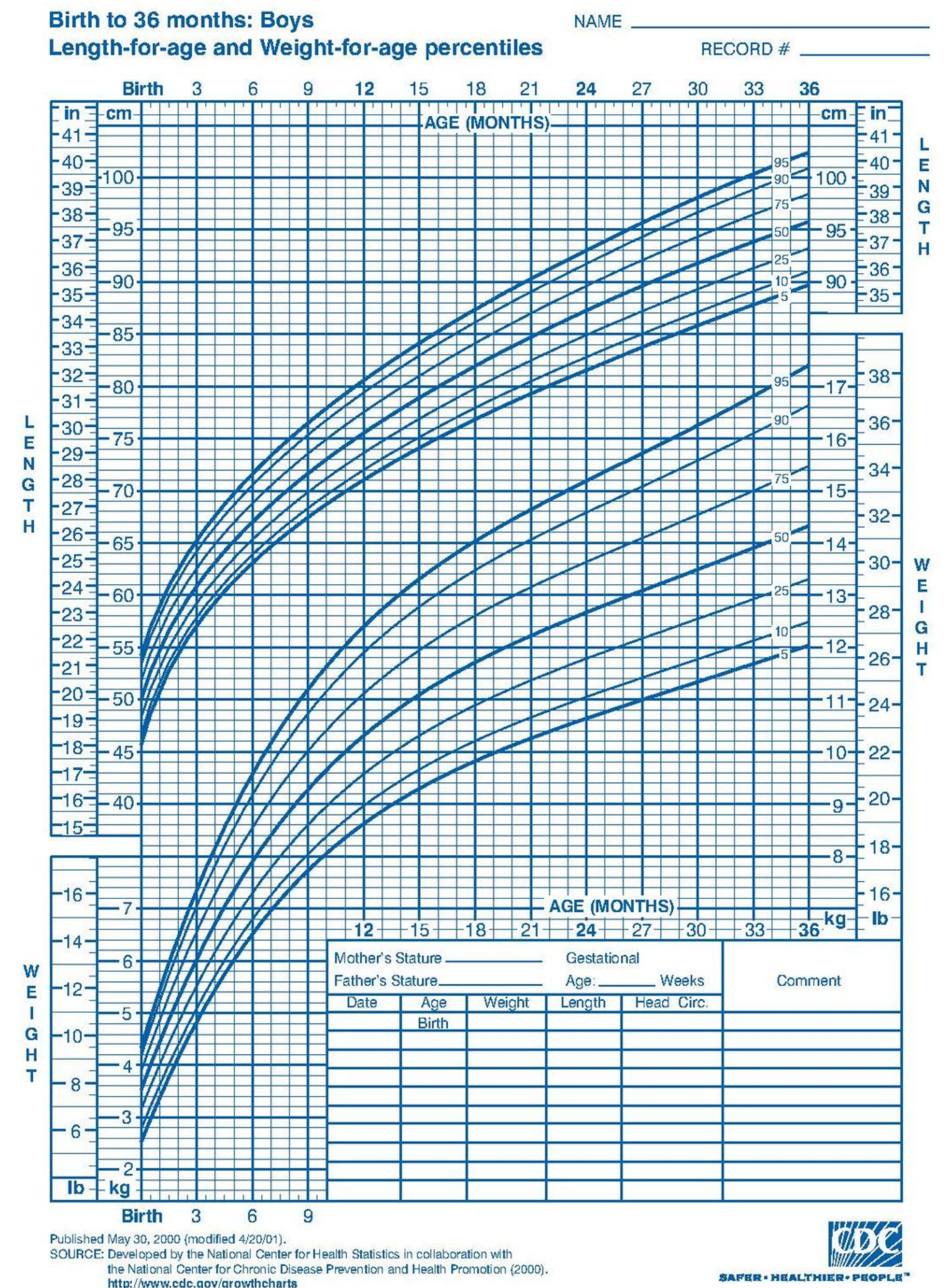
- Rate of publication and funding in TBI neuroimaging is accelerating but successful translation can be hampered by small sample sizes limiting generalizability
- Increasing understanding of the need for multi-site/multi-cohort analyses
- Data must be comparable however to avoid garbage-in/garbage-out





# Why is harmonization important for biomarker development?

- Standardization is necessary to make biomarkers usable clinically
  - Imagine every doctors office using different units of measurement - inches, cm, hands, bananas, etc.
- Historically there hasn't been much consideration of this with MRI
  - Disincentive for having data that could be combined





# Many sources of site effects

- Methodological sources

- Scanner platform - SNR/CNR, coil inhomogeneity
- Scan sequence - sensitivity to tissue differences, sensitivity to motion
- Acquisition procedure - task details, instructions, time of day, motion
- Postprocessing

- Biological

- Age
- Sex/Gender
- Severity/chronicity of condition - treatment, medication
- Background demographics - SES, race/ethnicity, genetics, environmental exposures
- Control samples
- Inclusion/exclusion criteria

# Prospective harmonization

- Synchronizing scan parameters prior to data collection
  - Sequences coordinated across vendors - not identical
  - Some sequences vary within individual within scanner
    - DWI/DTI, fMRI, ASL
    - Hydration, caffeine
  - Often use “human phantoms”
- Examples
  - ADNI
  - ABCD
  - TRACK-TBI
  - LIMBIC-CENC
  - CARE Consortium and CARE4Kids

## Neuroimaging Parameters

Siemens	Matrix	Slices	FOV	% FOV phase	Resolution (mm)	TR (ms)	TE (ms)	TI (ms)	Flip Angle (deg)	Parallel Imaging	MultiBand Acceleration	Phase partial Fourier	Diffusion Directions	b-values	Acquisition Time
T1	256 x 256	176	256 x 256	100%	1.0 x 1.0 x 1.0	2500	2.88	1060	8	2x	Off	Off	N/A	N/A	7:12
T2	256 x 256	176	256 x 256	100%	1.0 x 1.0 x 1.0	3200	565	N/A	Variable	2x	Off	Off	N/A	N/A	6:35
Diffusion fMRI														500 (6-dirs)	
														1000 (15-dirs)	
														2000 (15-dirs)	
	140 x 140	81	240 x 240	100%	1.7 x 1.7 x 1.7	4100	88	N/A	90	Off	3	6/8	96	3000 (60-dirs)	7:31
	90 x 90	60	216 x 216	100%	2.4 x 2.4 x 2.4	800	30	N/A	52	Off	6	Off	N/A	N/A	
Philips	Matrix	Slices	FOV	% FOV phase	Resolution (mm)	TR (ms)	TE (ms)	TI (ms)	Flip Angle (deg)	Parallel Imaging	MultiBand Acceleration	Half Scan Factor	Diffusion Directions	b-values	Acquisition Time
T1	256 x 256	225	256 x 240	93.75%	1.0 x 1.0 x 1.0	6.31	2.9	1060	8	1.5 x 2.2	Off	N/A	N/A	N/A	5:38
T2	256 x 256	256	256 x 256	100%	1.0 x 1.0 x 1.0	2500	251.6	N/A	90	1.5 x 2.0	Off	N/A	N/A	N/A	2:53
Diffusion fMRI														500 (6-dirs)	
														1000 (15-dirs)	
														2000 (15-dirs)	
	140 x 140	81	240 x 240	100%	1.7 x 1.7 x 1.7	5300	89	N/A	78	Off	3	0.6	96	3000 (60-dirs)	9:14
	90 x 90	60	216 x 216	100%	2.4 x 2.4 x 2.4	800	30	N/A	52	Off	6	0.9	N/A	N/A	
GE	Matrix	Slices	FOV	% FOV phase	Resolution (mm)	TR (ms)	TE (ms)	TI (ms)	Flip Angle (deg)	Parallel Imaging	MultiBand Acceleration	Phase partial Fourier	Diffusion Directions	b-values	Acquisition Time
T1	256 x 256	208	256 x 256	100%	1.0 x 1.0 x 1.0	2500	2	1060	8	2x	Off	Off	N/A	N/A	6:09
T2	256 x 256	208	256 x 256	100%	1.0 x 1.0 x 1.0	3200	60	N/A	Variable	2x	Off	Off	N/A	N/A	5:50
Diffusion fMRI														500 (6-dirs)	
														1000 (15-dirs)	
														2000 (15-dirs)	
	140 x 140	81	240 x 240	100%	1.7 x 1.7 x 1.7	4100	81.9	N/A	77	Off	3	5.5/8	96	3000 (60-dirs)	7:30
	90 x 90	60	216 x 216	100%	2.4 x 2.4 x 2.4	800	30	N/A	52	Off	6	Off	N/A	N/A	



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# Phantom harmonization

## CHIPS Project

- Use of novel phantom objects where models of tissue with known properties can be used to assess scanner accuracy
- CHIPS project currently working to use phantoms across VAs to improve scanner accuracy and data comparability
  - Example: anisotropic diffusion can be measured with hollow 6-10  $\mu\text{m}$  fibers arranged to mimic white matter tracts
  - Measurements can be compared to known diffusion properties and correction algorithm can be applied



Phantom Laboratory



Psychology Software Tools

# Ground truth

- Phantom harmonization - closest to ground truth, but it's not biological tissue
- Prospective sequence harmonization with traveling human phantoms - next best thing
- But what about retrospective harmonization? How to identify ground truth?
- No single answer yet - common approach is to model a known biological effect before and after harmonization to ensure it is preserved
- Room for improvement here!



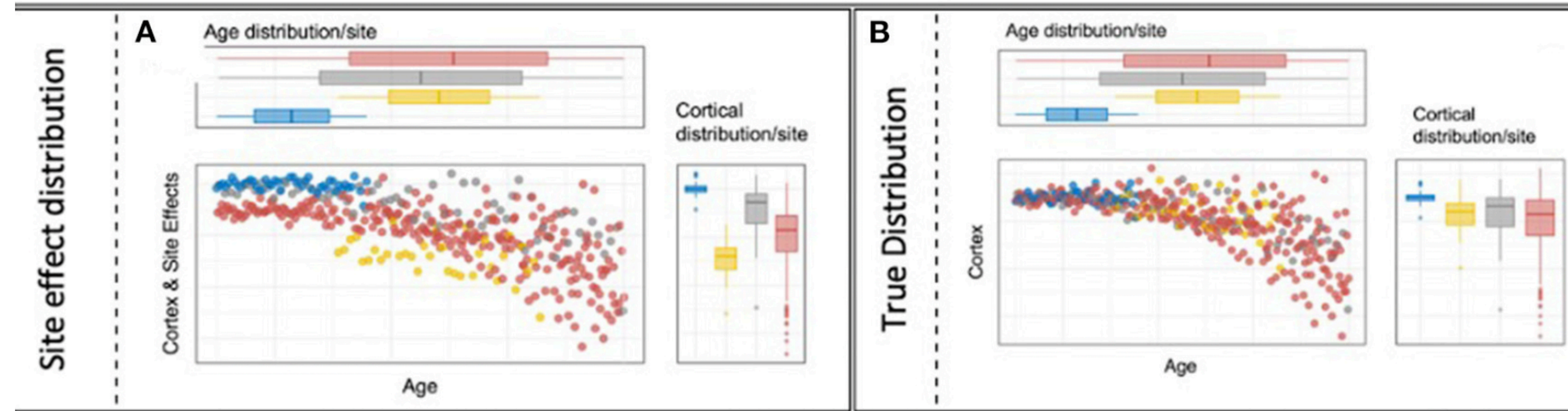
# Retrospective harmonization techniques

- Next slides review several approaches for statistical harmonization
- Key take-away is how do the outputs vary

# Retrospective harmonization

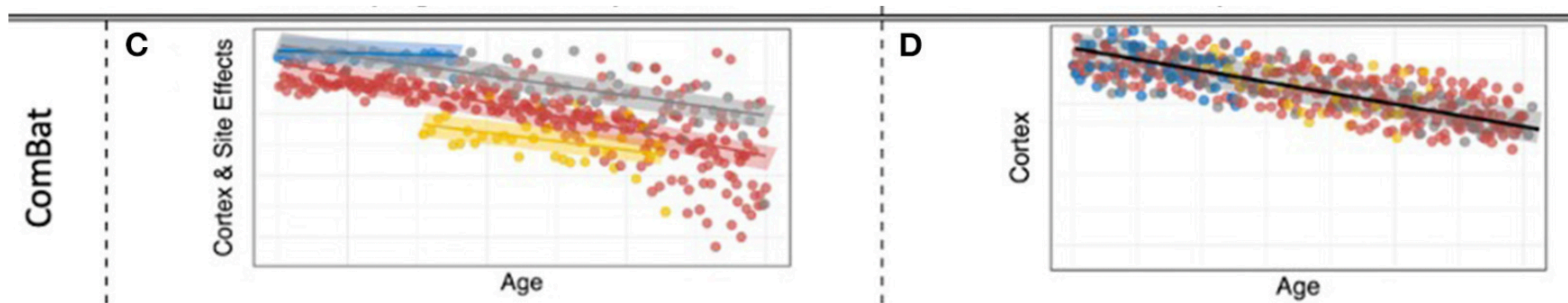
## ComBat

- Linear adjustment of site means
- Scaling site variance differences
- Can preserve specific covariate effects



Underlying estimation process

Output

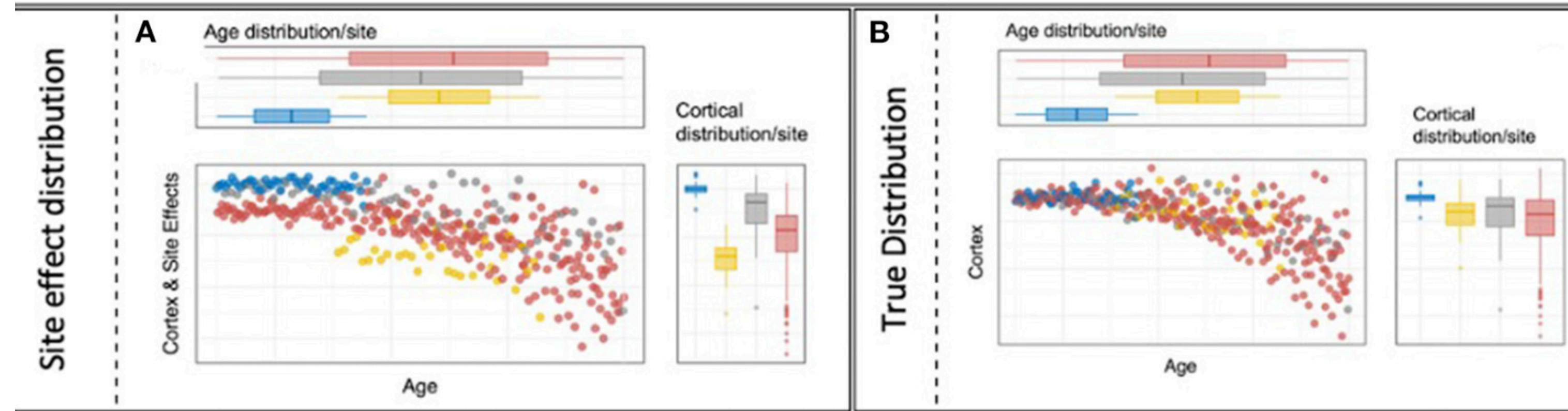




# Retrospective harmonization

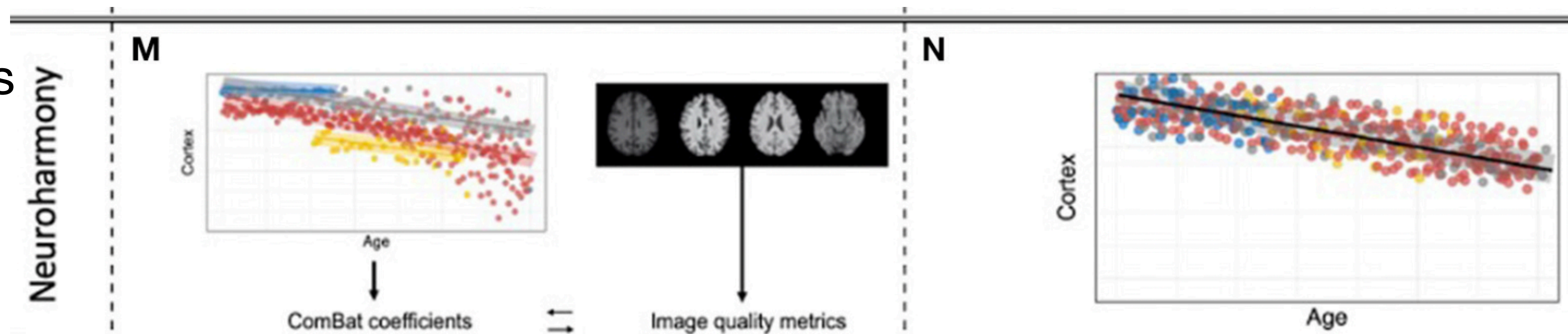
## Neuroharmony

- Calculate image quality metrics
- Use these as predictors in ComBat
- Apply coefficients to imaging features



Underlying estimation process

Output

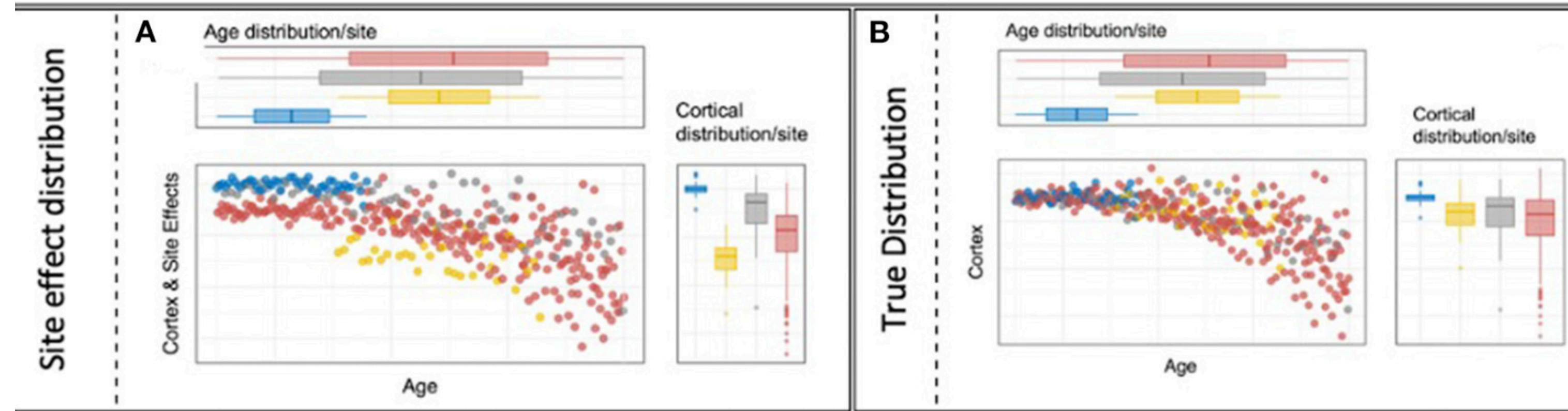




# Retrospective harmonization

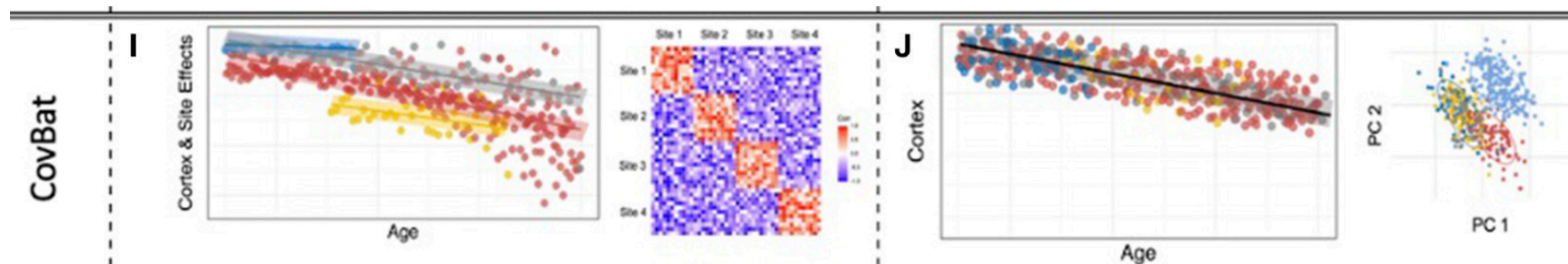
## CovBat

- 2 runs of ComBat
  - First as usual
  - Second on a PCA of the residuals from the first to harmonize the covariance



Underlying estimation process

Output

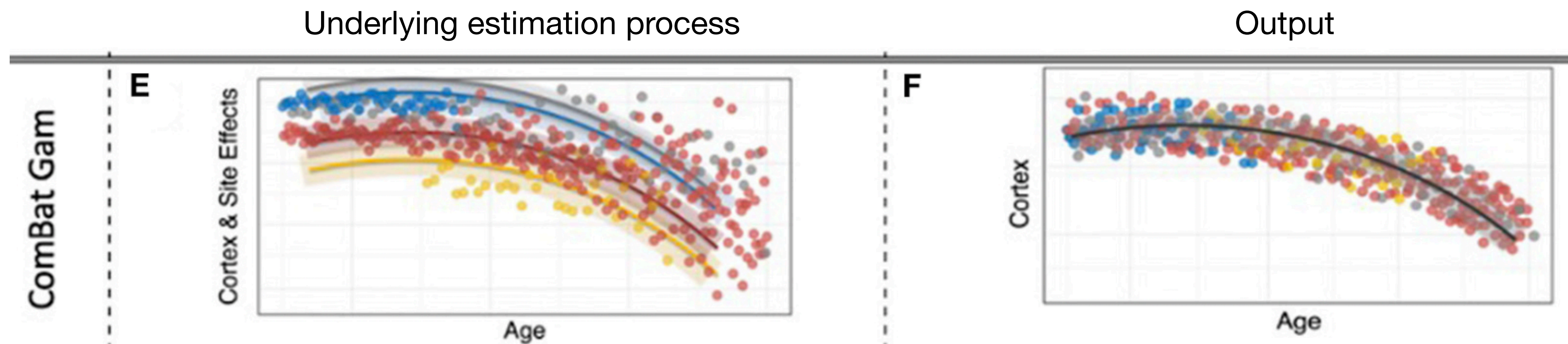
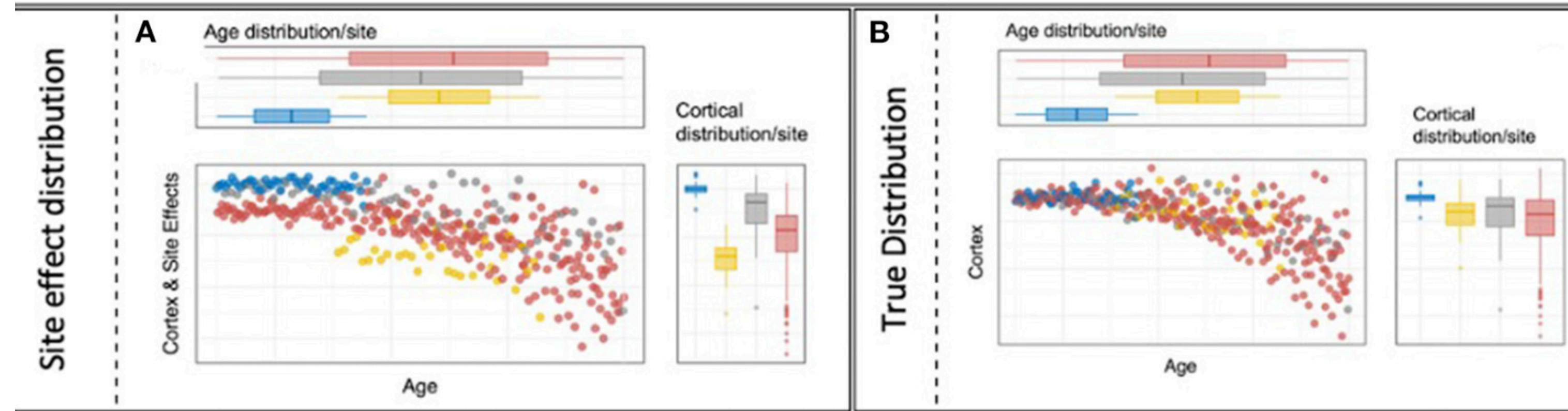




# Retrospective harmonization

## ComBat-GAM

- Similar to ComBat
- Non-linear adjustment



There are many more variations on ComBat, including some that use federated learning so that raw data sharing isn't required

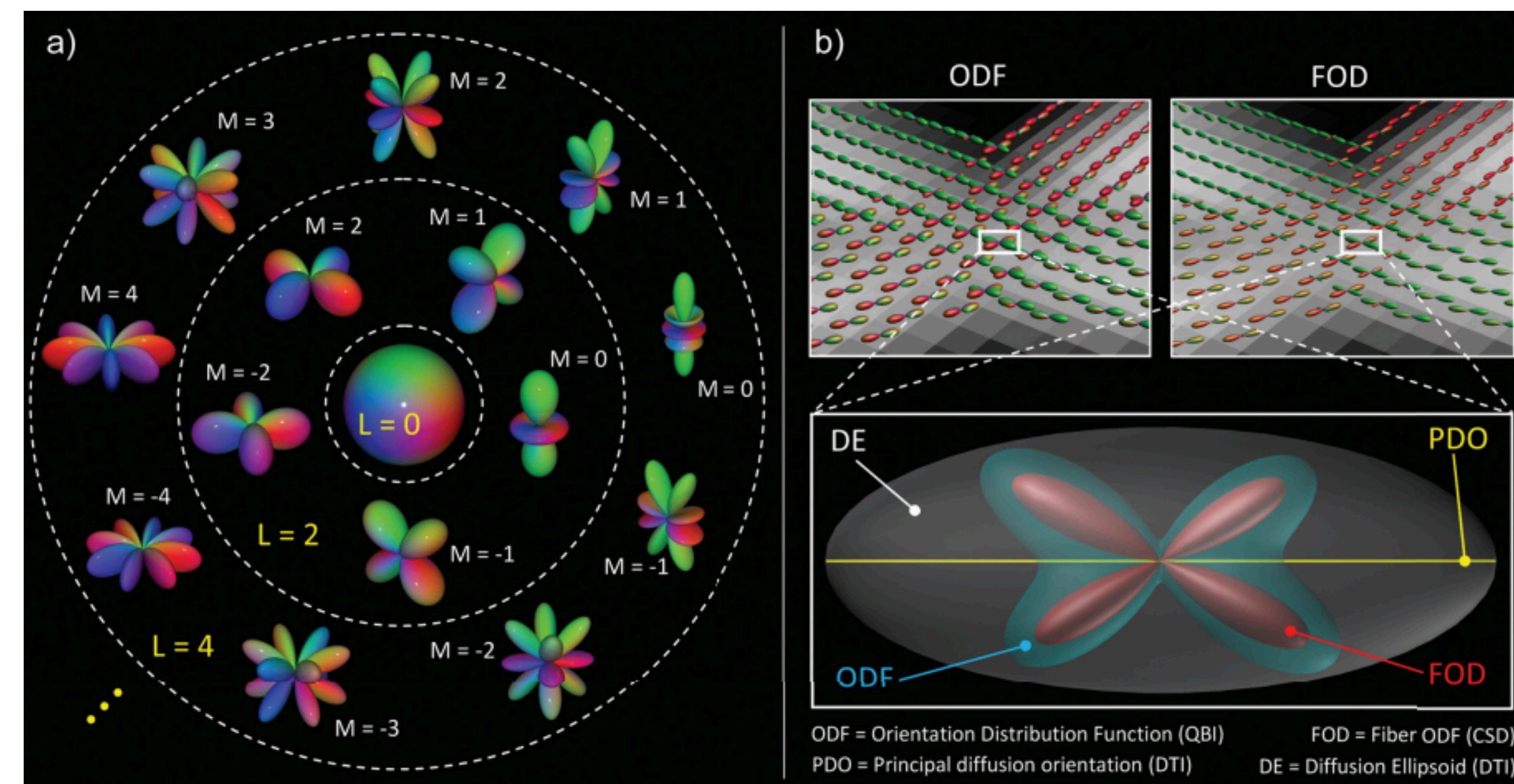
# When to harmonize

- Raw imaging data
- Derived imaging metrics
- Summary imaging metrics



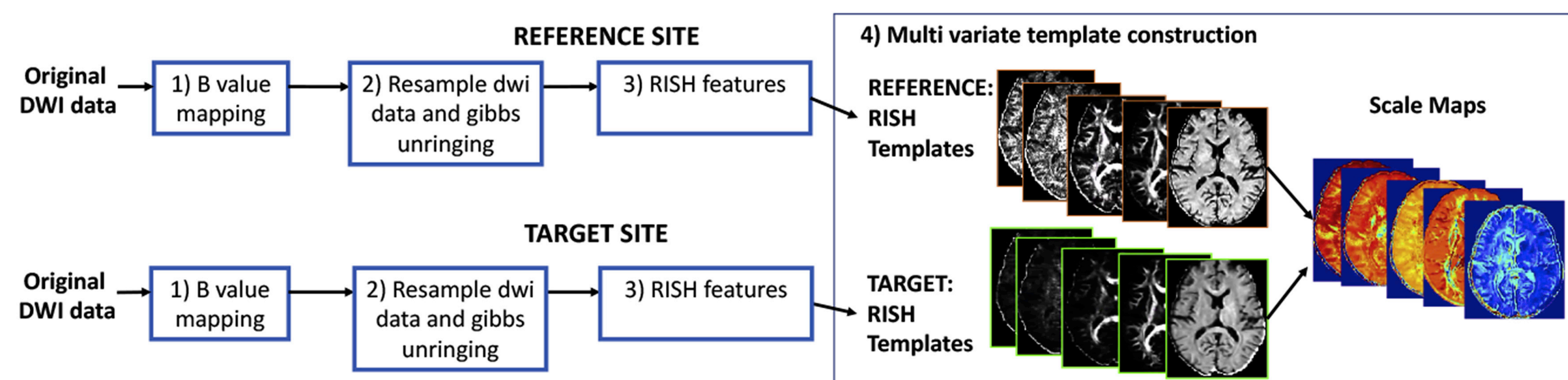
# Harmonization of raw diffusion MRI

- Matched controls
- Scale  $b$ -values
- Upsample data to standardize voxel resolution
- Signal at each voxel is represented by spherical harmonics (equations to describe a sphere)
- Harmonics can be scaled and applied to dataset

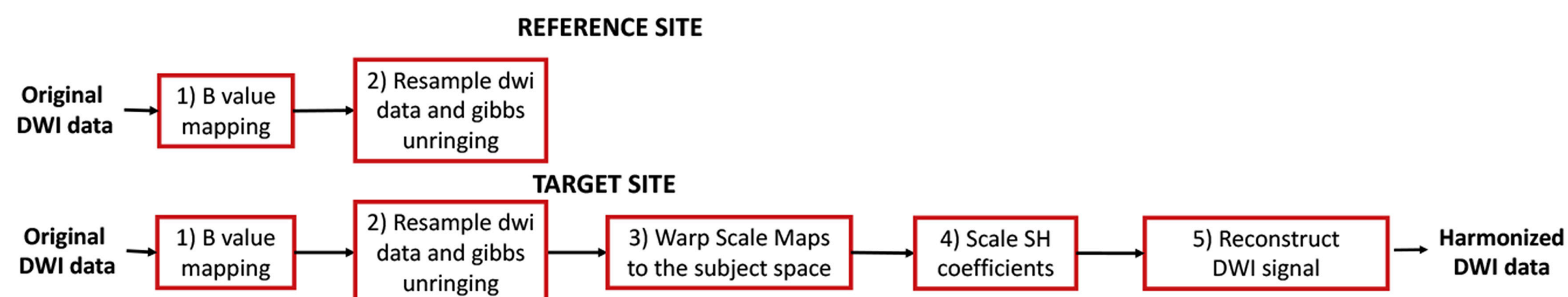


Leemans, Diffusion MRI 2010

**(a) Learning inter-site differences only from training subjects:**



**(b) Applying the learned inter-site differences to harmonize all subjects:**



Cetin-Karayumak et al., NIMG 2019



# When to harmonize

- Raw imaging data
- Derived imaging metrics
- Summary imaging metrics

**A Before harmonization**

**B Matrix harmonization**

**C Parameter harmonization**

**Global efficiency**

$r = 0.16, p < 0.001$

$r = 0.38, p < 0.001$

$r = 0.44, p < 0.001$

Global efficiency

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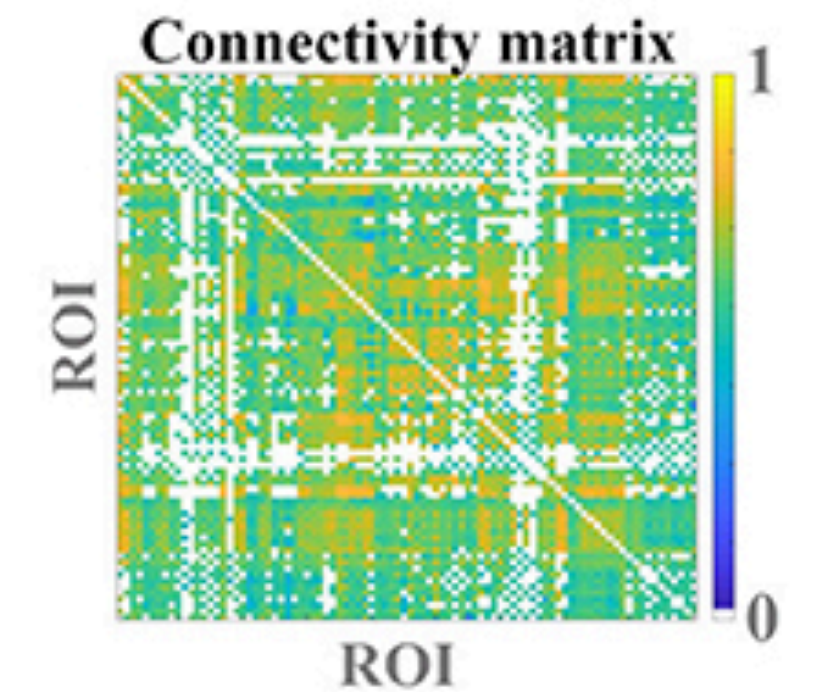
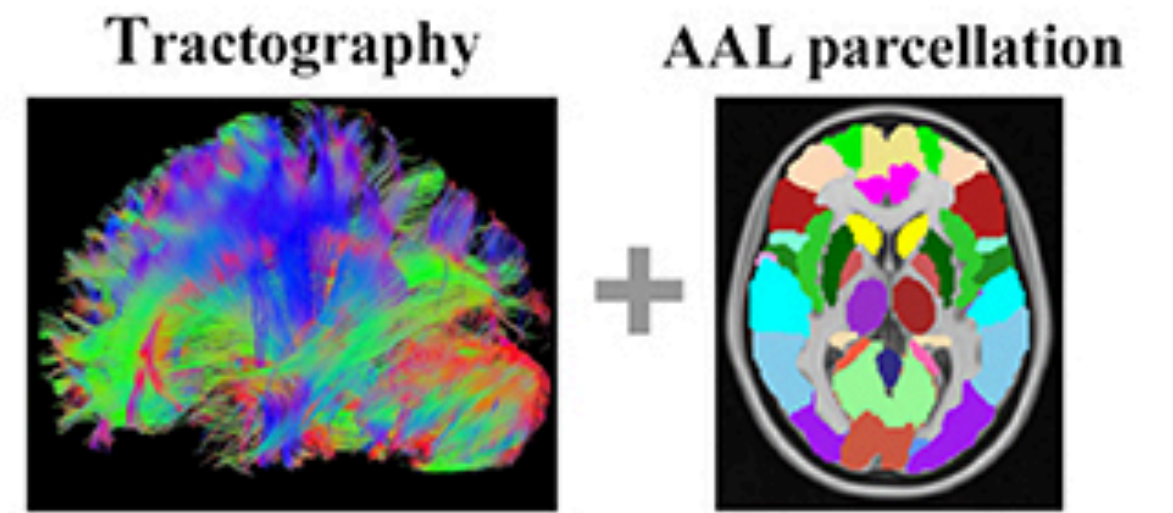
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**A Before harmonization**



**Global network parameters**



**Site**

- Calgary
- Edmonton
- Montreal 1
- Montreal 2
- Ottawa
- Vancouver



# Summary

- Why is this important for biomarker development?
  - We should be able to leverage the vast amount of data that has been collected already to develop normative databases for a whole range of imaging metrics
- There have been tremendous advances in this area in the last decade
  - Technical - better computer hardware makes computationally intensive algorithms and programs feasible
  - Sociological - increasingly willingness and enthusiasm for collaboration and data sharing
    - Federal archives like FITBIR and NDA support these efforts

**Each advancement brings us closer to the goal of being able to place an individual scan in context, furthering precision medicine efforts**

# References

- Bayer, Johanna MM, et al. “Site effects how-to and when: An overview of retrospective techniques to accommodate site effects in multi-site neuroimaging analyses.” *Frontiers in Neurology* 13 (2022).
- Cetin-Karayumak, Suheyla, et al. “Retrospective harmonization of multi-site diffusion MRI data acquired with different acquisition parameters.” *Neuroimage* 184 (2019): 180-200.
- Onicas, Adrian I, et al. “Multisite harmonization of structural DTI networks in children: An A-CAP study.” *Frontiers in Neurology* 13 (2022).