2.2 Replacing Cesium-137 Irradiators at University of California, Los Angeles

Gamma-irradiators, X-irradiators, and Radiobiology

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The University of California owns (owned) 47 Cesium or Cobalt irradiators

10 campuses and 5 medical centers

Cesium 137

- Research irradiators 36
- Medical- blood irradiators- 6

Cobalt 60

- Research 2
- Medical-gamma knives 3



223,000 staff and faculty ~ 273,000 students

NNSA (National Nuclear Security Administration) Incentives

One γ -irradiator removed and replaced with one x-irradiator => \$135K Two γ -irradiators removed and replaced with one x-irradiator => \$203K Three γ -irradiators removed and replaced with one x-irradiator => \$216K Four γ -irradiators removed and replaced with one x-irradiator => \$230K

UC President Management Decision

A "UC Decision Memo" was written analyzing the scope of the issue for the University and it proposed:

Dedicated Project Management – A dedicated person to manage the program.

Technical Conferences – Hold two conferences to discuss the technical issues of converting from Cesium irradiators to x-ray irradiators.

Faculty Working Group – Form a Faculty Technical Working Group to provide technical recommendations on how to proceed.

Centralized purchasing – Streamline purchasing of the new x-ray irradiators by centralizing the process and seeking best prices.

The plan was endorsed and presented to senior management.

| Campus | Location | Clin/Res | Use | Identifier | Replacement X-irradiator |
|--------|------------|----------|------------------|--------------|-----------------------------|
| UCLA | BSRB | Research | Animal | Mark 1-68A | XRAD 320 |
| UCLA | CHS | Research | Animal | GammaCell 40 | XRAD 320 |
| UCLA | CHS | Research | Animal | Mark 1-68A | |
| UCLA | CHS | Research | Cell/Animal | Mark 1-30 | |
| UCLA | CHS | Research | Dosimetry/Animal | T-1000 | |
| UCLA | Rehab Cntr | Research | Cell | GammaCell 10 | |
| UCLA | TLSB | Research | Animal/Cell | Mark 1-68A | RS2000 |
| | | | | | |
| _ | | | | | |
| UCLA | Hospital | Clinical | Blood | | One for one |
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RBE = Dose of Cs-137 γ -rays to produce a given biological effect

Dose of x-rays to produce the same biological effect

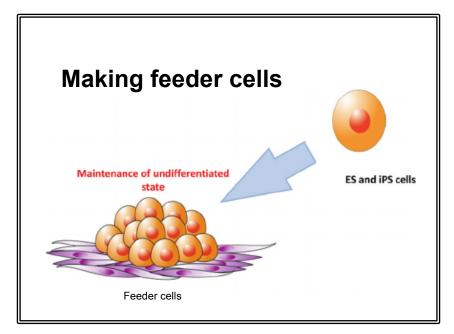
| x-ray energy | RBE to CS- 137 | Relative dose increase | system | endpoint | citation | notes | Model |
|------------------------------|-------------------|------------------------------|--------------------|---|--------------------------|--|---------|
| 320 kV (1mm Cu HVL) | | 1.16 | Bone marrow | Clonogenic growth post in vivo IR | Belley et al. 2015 | | animals |
| 320 V (4mm Cu HVL) | | 1.07 | Bone marrow | Clonogenic growth post in vivo IR | Belley et al. 2015 | | animals |
| 320 kV | 0.763 | | Splenocytes TBI | cytotoxicity | Scott et al. 2013 | | animals |
| 320 kV | 1.346 | | Bone marrow TBI | cytotoxicity | Scott et al. 2013 | | animals |
| 160 kV | See note | | Bone marrow | Bone marrow transplant reconstitution | Gibson et al. 2015 | Due to the statistically significant variability in B, T, myeloid cell reconstitution between the X-ray and 137Cs sources of irradiation, we accept the null hypothesis. We conclude that although both sources were efficient at ablating endogenous bone marrow sufficiently to enable stem cell engraftment, there are distinct physiologic responses that should be considered prior to choosing the optimal source for use in a study. In addition, irradiation using the 137Cs source was associated with lower overall morbidity. | animals |
| 300 kV (1.65mm Cu HVL) | 1.11 | | Gut | Jejunal crypt assay | Fu et al. 1979 | Survival of 100 cells/circumference ten 1.56 Gy fractions | animals |
| 300 kV (1.65mm Cu HVL) | 1.08 | | Gut | Jejunal crypt assay | Fu et al. 1979 | Survival of 10 cells/circumference for ten 1.56 Gy fractions | animals |
| 300 kV (1.65mm Cu HVL) | 1.07 | | Gut | Jejunal crypt assay | Fu et al. 1979 | Survival of 1 cells/circumference for ten 1.56 Gy fractions | animals |
| 300 kV (1.65mm Cu HVL) | 1.00 | | Gut | Jejunal crypt assay | Fu et al. 1979 | Survival of 100 cells/circumference for a single fraction of 11.36 Gy | animals |
| 300 kV (1.65mm Cu HVL) | 1.00 | | Gut | Jejunal crypt assay | Fu et al. 1979 | Survival of 10 cells/circumference for a single fraction of 11.36 Gy | animals |
| 300 kV (1.65mm Cu HVL) | 1.08 | | Gut | Jejunal crypt assay | Fu et al. 1979 | Survival of 1 cells/circumference for a single fraction of 11.36 Gy | animals |
| 320 kV (HVL 1mm Cu) | 1.5 | | HBEC-13 | Cytotoxicity via MTT | LRRI (Scott et al. 2013) | | cells |
| 320 kV (HVL 1mm Cu) | 1.6 | | HBEC-2 | Cytotoxicity via MTT | LRRI (Scott et al. 2013) | | cells |
| 320 kV (HVL 3.7mm Cu) | 1.2 | | HeLa | Cytotoxicity via MTT | LRRI (Scott et al. 2013) | | cells |
| 320 kV (HVL 3.7mm Cu) | 1.5 | | A549 | Cytotoxicity via MTT | LRRI (Scott et al. 2013) | | cells |
| 300 kV (HVL 3mm Cu) | Approx 1.23 | | C57BL/6 | LD50/30 | UCLA radonc | | animals |

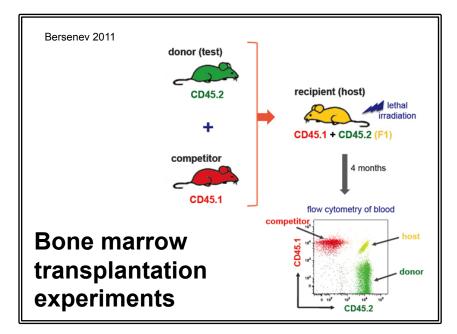
UC-wide Survey Results

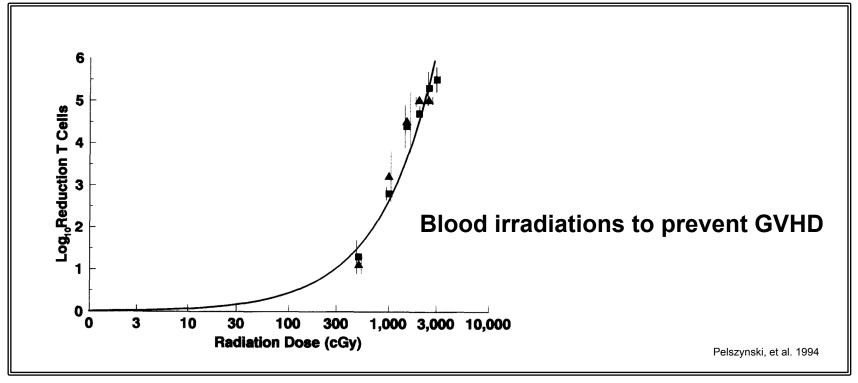
Approximately half the studies involve *in vitro* (cells) and half involve *in vivo* (rodents) irradiations.

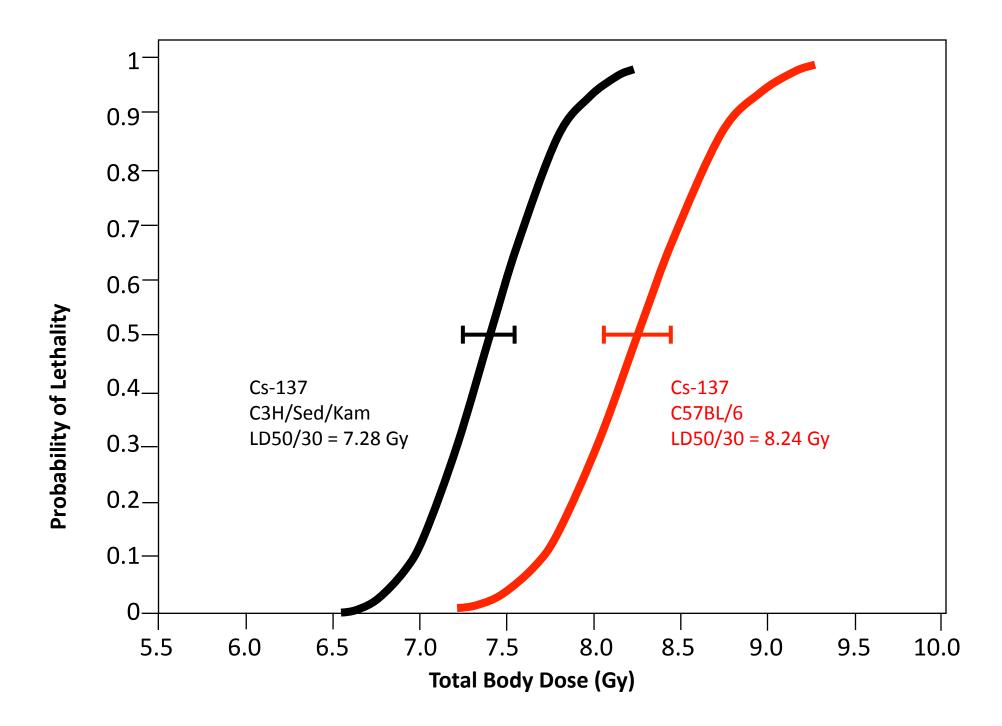
The largest single proportion (41%) of the *in vitro* irradiations was for production of feeder cells to support growth of growth-factor-dependent cells.

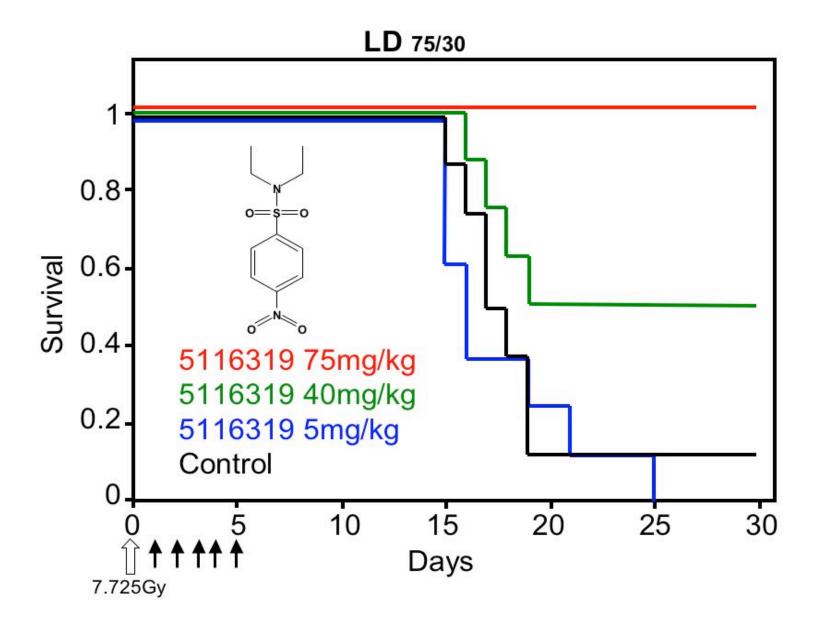
The largest single proportion (37%) of the *in vivo* irradiations was for bone marrow ablation in preparation for transplantation experiments.

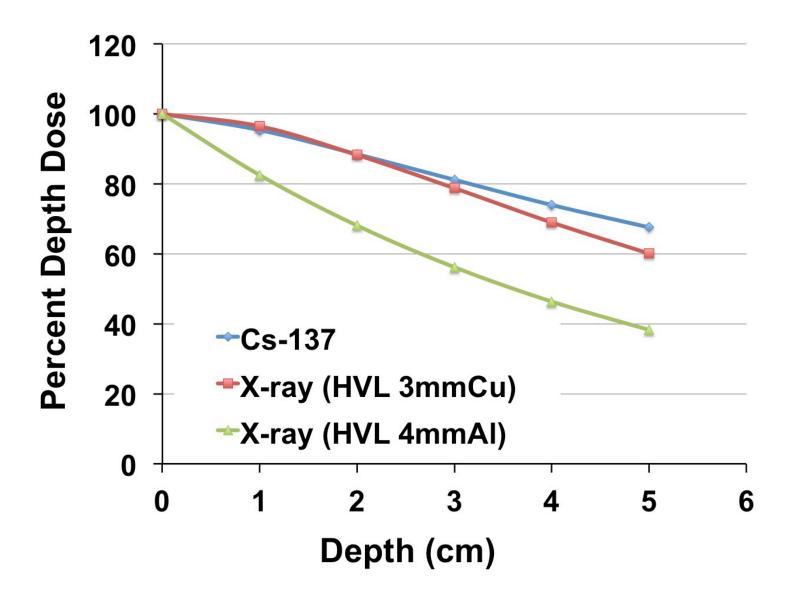


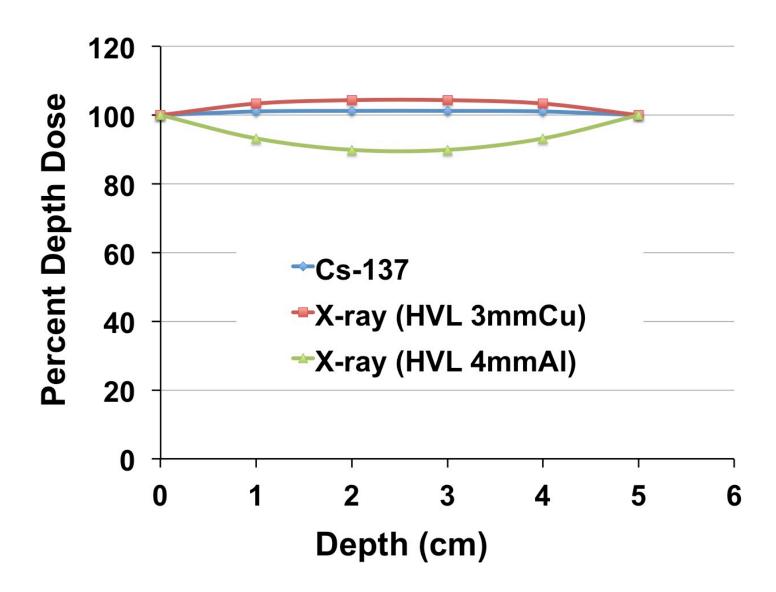


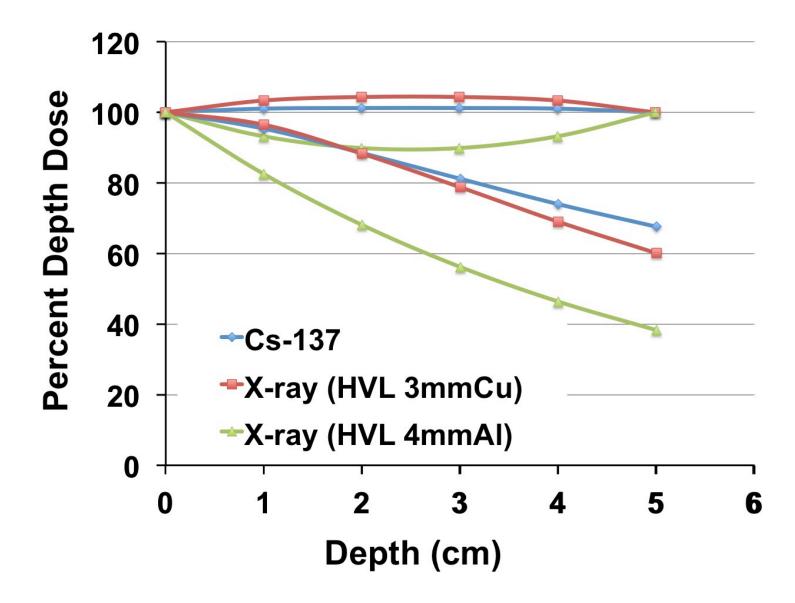












Radiobiological Considerations or Not

Biology is a dynamic system

There is always a response

Biological dose ≠ physical dose

In general, x-rays (energies equal to or below 320 kV) are more biologically effective than Cs-137 gamma rays suggesting that lower doses of x-rays will be required to achieve the same biological endpoint as Cs-137 gamma rays. Conversely, less penetration in some targets may reduce dose effects.

Different endpoints => different RBE's

It is difficult to provide a simple conversion factor for equating x-ray effects to Cs-137 effects because RBE depends on multiple factors including x-ray peak energy, x-ray energy spectrum (filtration), biological system, endpoint, etc.

• Different IR sources & conditions => different cellular responses

Standardization – Unlike the single gamma energy of Cs-irradiators, output energies of the x-irradiators cited in the literature are diverse due to variations in x-ray tubes and filtration utilized; in some cases, the quality of the beam (HVL) is not described.

Geometry can make a difference

ID of the IR may not matter much or at all in some cases

Each experiment will need to be individually calibrated when converting from Cs-irradiators to x-irradiators and the effort and resources required will depend on the precision of the effect desired. For example, in cases where inactivation of support cell proliferation or unwanted cell activity is desired, as in the case of production of feeders, the specificity of the absolute dose may not be as critical as ascertaining animal lethality dose.

UC Source Replacement Faculty Working Group (WG) Recommendations:

- X-ray irradiators can replace cesium irradiators in many applications. There are likely some exceptions though, such as the need for very high radiation doses or radiation exposures over a period of days, and research specifically requiring high energy gamma radiation.
- Every established laboratory/investigator needs to empirically assess the effects to their studies of converting from cesium to x-rays specific with their own comparison studies.

Slide courtesy of Carolyn MacKenzie University of California, Berkeley

Lessons Learned for a Smooth Transition

A collaborative approach is best! Do not force researchers to switch – make them a part of the decision making process.

Offer money incentives, options to upgrade research equipment and support for comparison studies.

Talk to the researchers about their research – do not shut down research but plan for exceptions.

Take a phased approach- acceptance will come with time.